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# 1 **Fluorescein isothiocyanate chitosan nanoparticles in oral drug delivery studies**

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## 6 **Keywords**

7 Fluorescein isothiocyanate; chitosan nanoparticles; drug bioavailability; oral delivery.

## 8 **Abstract**

9 Oral administration of drugs is one of the most patient-friendly drug delivery routes. However, drug  
10 bioavailability via the oral route remains poor due to the harsh gastrointestinal environment. In recent  
11 years, many nanocarriers have been designed to overcome this limitation. Among those, chitosan  
12 nanoparticles (ChNPs) have proved to be quite a popular choice. Here, we highlight the use of  
13 fluorescein isothiocyanate-tagged ChNPs (FITC@ChNPs) as an invaluable tool to monitor the fate  
14 of ChNPs encapsulating oral drugs, leading to an in-depth understanding of drug biodistribution and,  
15 in turn, shedding a light on ways to improve bioavailability.

16

## 17 **Use of Chitosan Nanoparticles in Oral Drug Delivery**

18 Oral administration of drugs offers several benefits over other systemic drug delivery routes.  
19 Generally, the oral route is considered to be convenient, relatively safe and economically efficient.  
20 Additionally, this route often leads to improved patient compliance and lifestyle when compared to  
21 other delivery routes such as intravenous (IV) injection, which may present dermal pain and  
22 discomfort [1]. However, many peptide drugs and anti-cancer agents show several challenges upon  
23 oral administration, due to the low water solubility, unsuitable transport across the gastrointestinal  
24 (GI) mucosa, enzymatic degradation, or low pH deactivation. Moreover, the presence of tight  
25 junctions (TJs) and efflux pumps (such as P-glycoprotein) on enterocytes prevent both the  
26 paracellular and transcellular transports of any drugs. As a result, a suitable concentration of the drug  
27 in the blood stream, and in turn a suitable level of bioavailability, is not achieved [2,3]. In this context,  
28 many nanocarriers have been developed with the aim of improving the bioavailability of orally  
29 administered drugs. Among these, chitosan nanoparticles (ChNPs) have been extensively employed.  
30 as oral drug delivery systems as these can protect the encapsulated drug from GI degradation and  
31 promote its absorption across the GI mucosa [4]. The ChNPs provide researchers with the opportunity  
32 to functionalise their surface to obtain longer circulating and/or targeted delivery systems [4].  
33 However, possessing a tool that enables researchers to monitor the fate of drug loaded ChNPs allows  
34 an in-depth understanding of the biodistribution of these ChNPs and drives better designs of NPs,  
35 which in turn enable improvements of the oral bioavailability of drugs. Here, we highlight the  
36 usefulness of fluorescein isothiocyanate-tagged ChNPs (FITC@ChNPs) as a tool to track the fate of  
37 ChNPs and monitor drug biodistribution and bioavailability.

38 Chitosan is a glucosamine-based biopolymer, which is formed from naturally occurring chitin  
39 and characterized by a multitude of biological and pharmacological features, including wound  
40 healing, antioxidant and antibacterial properties, biodegradability, and biocompatibility [5]. It is  
41 produced by incomplete alkaline deacetylation of chitin, leading to enhanced water solubility under

42 acidic conditions. The aqueous solubility is due to the protonation of the free primary amino groups  
43 ( $pK_a$  of the resulting  $-NH_3^+ = \sim 6.5$ ) when chitosan is dissolved in weakly acidic solutions [5]. This  
44 behaviour also accounts for the mucoadhesive properties of chitosan: electrostatic bonds are  
45 established between the protonated amino groups and the negatively charged sialic acid anions of  
46 mucin glycoproteins, lining the mucous membrane of internal organs.

47 Chitosan is used in a variety of applications, for instance in the production of drug nano  
48 vehicles, including micelles, and NPs [5]. The mucoadhesive property is valuable in achieving  
49 acceptable oral bioavailability since it allows ChNPs to adhere to the GI mucosa, increasing cellular  
50 absorption through adsorptive endocytosis and decreasing the required drug dosing frequency [6].  
51 Moreover, the protonated amino groups can open TJs between epithelial cells, enhancing the  
52 paracellular transport of drugs [7]. However, this property is limited to the duodenum where the pH  
53 (6 - 7) is close to the  $pK_a$  of chitosan [7]. In other pH ranges, chitosan loses its mucoadhesive  
54 properties and dissolves out [8]. To circumvent this, modifications of chitosan structure are needed.  
55 The presence of functional groups allows the chemical modification of chitosan with a variety of  
56 biomolecules such as methylcellulose phthalate (HPMCP) [1], thiol groups [9], methyl groups [10],  
57 and fluorescent molecules including FITC [11]. Such modifications increase the solubility and  
58 mucoadhesivity of chitosan, protect it from gastric dissolution [4], and allow ChNPs tracking across  
59 the GI tract using a fluorimeter.

60 ChNPs are nanosized colloids that can be easily produced in aqueous media by simple  
61 methods such as ionic gelation [12]. Owing to their size, ChNPs have been shown to be able to cross  
62 biological membranes, such as the intestinal epithelium, yielding a high drug accumulation at the  
63 target site. Moreover, they preserve the enclosed therapeutic agent from degradation, increasing its  
64 bioavailability and, in turn, altering its pharmacokinetics [12]. The use of ChNPs loaded with drugs  
65 for oral use in clinical trials is desirable as it could lead to significant improvements over conventional  
66 drug delivery for diabetes management or the treatment of site-specific tumours.

## 67 **Fluorescein Isothiocyanate-labelled Chitosan Nanoparticles**

68 ChNPs conjugated with fluorescent dyes are extensively used in biomedical applications such  
69 as cellular uptake studies and cellular imaging where owing to the added fluorescent feature, the  
70 intracellular and extracellular route of ChNPs can be efficiently tracked [13]. Nonetheless, the use of  
71 fluorescent NPs can pose several challenges. For instance, nonspecific detection can occur if the  
72 fluorophore is physically adsorbed on the surface of NPs. If the fluorophore is covalently conjugated  
73 to the drug delivery vehicle, its dissociation can be impeded during cellular uptake experiments or  
74 storage [13]. Several fluorophores such as lissamine-rhodamine and Cy5.5 have been conjugated to  
75 chitosan backbone so to allow the *in vitro* tracking of ChNPs. However, most of these organic  
76 fluorescent dyes show several limitations such as photobleaching, low signal intensity, toxicity, and  
77 poor solubility in water [11].

78 The conjugation of chitosan to FITC yields FITC@Ch and relies on a thiourea linkage, formed  
79 between the isothiocyanate group ( $R-N=C=S$ ) on FITC and the primary amine groups ( $-NH_2$ ) on  
80 chitosan (Figure 1a). The conjugation reaction prevents the dissociation of the fluorescent probe,  
81 helping with quantification and tracking of the NPs [14]. The use of FITC presents several  
82 advantages, including the ease of conjugation to chitosan, solubility in water, photostability, good  
83 biocompatibility along with intense and stable fluorescence emission [11] that allows easy detection  
84 of small NPs. Furthermore, the properties of ChNPs are not compromised by the presence of FITC  
85 and FITC@ChNPs are widely reported in the literature to track and investigate biodistribution of  
86 ChNPs in the GI tract [14] as these can be easily and rapidly quantified by fluorimetry (Figure 1b).  
87 However, the major challenge in using FITC@ChNPs concerns the purity of the conjugates since a  
88 very low purity of FITC@Ch can lead to a misinterpretation of results. Moreover, quantification of  
89 FITC@ChNPs by fluorimetry is only possible if a suitably accurate and sensitive method is developed  
90 [13].

## 91 **FITC@ChNPs to increase bioavailability and biodistribution of various oral payloads**

92            Investigations involving FITC@ChNPs can help find a suitable GI biodistribution of ChNPs,  
93 in turn increasing drug bioavailability (Figure 1b). Below we discuss recent key *in vitro*, *ex vivo* and  
94 *in vivo* studies involving FITC@ChNPs that aimed at enhancing the oral bioavailability of drugs.

### 95 *Protein payloads*

96            Protein drugs and vaccines play key roles in treating or managing numerous diseases, but upon  
97 oral administration they face several limitations including degradation by proteolytic enzymes and  
98 poor GI permeability [4]. For instance, insulin is a peptide hormone commonly used in diabetes  
99 management, but has poor patient compliance due to the requirement of daily subcutaneous injections  
100 [1]. To increase insulin oral bioavailability and biodistribution, several investigations have been  
101 performed employing insulin loaded on FITC@ChNPs. In a study conducted by Makhlof *et al.* [14],  
102 rats were fed with insulin loaded FITC@ChNPs cross-linked with HPMCP, a pH-sensitive polymer  
103 widely used to coat enteric capsules, protecting the encapsulated drug from gastric degradation [1].  
104 FITC allowed the visualization of drug loaded NPs in the intestinal mucosa. A stronger fluorescence  
105 in the GI mucosa was noticed for rats treated with FITC@ChNPs cross-linked with HPMCP  
106 compared to the control (FITC@ChNPs) leading to the conclusion that cross-linking with HPMCP  
107 increased mucoadhesion and penetration of the insulin-loaded NPs through the intestine, in turn  
108 improving the peroral delivery of insulin. Cross-sections of the intestinal mucosa were further  
109 analysed by confocal microscopy and an interaction of NPs with the membrane was revealed,  
110 meaning that NPs were not trapped in the gel layer [14]. He *et al.* [1] evaluated the impact that the  
111 size of ChNPs has on the transport and absorption of the loaded insulin in Caco-2 cell monolayers  
112 (human intestinal cell line widely employed to investigate the ability of drug loaded NPs to cross the  
113 GI epithelium). This experiment was performed by labelling ChNPs with FITC so as to observe in  
114 real time the behaviour of the resulting NPs. Results showed that smaller NPs (45 nm) surmounted  
115 the epithelial barrier faster than larger ones (115 nm), as shown by the stronger fluorescent intensity  
116 given by the treatment with small FITC@ChNPs. Confocal images illustrated that the small NPs

117 induced a transient and reversible opening of TJs between enterocytes, increasing the concentration  
118 of the released insulin at the site of absorption, which is a desirable effect in targeted drug delivery  
119 [1]. Another recent work employed FITC to assess the mucoadhesive properties and biodistribution  
120 of thiolated ChNPs for the oral delivery of insulin [9]. *In vivo* biodistribution studies were performed  
121 after oral administration of insulin loaded thiolated FITC@ChNPs to rats. A fluorescent layer was  
122 noticed above the microvilli of the GI mucosa, suggesting a suitable biodistribution of orally delivered  
123 insulin loaded FITC@ChNPs because of the enhanced mucoadhesivity conferred by the thiol groups  
124 on chitosan [9]. Moreover, cellular uptake of thiolated ChNPs was assessed in Caco-2 cells by means  
125 of FITC's fluorescence intensity which showed that thiolated ChNPs were efficiently engulfed by  
126 cells.

127 Vaccine studies have also used FITC labelled ChNPs to gain insights on the biodistribution  
128 profiles. For example, Liu *et al.* [15] employed FITC to label oleoyl-carboxymethyl Ch (CmCh) and  
129 generate NPs that acted as oral protein carriers of a bacterial antigen (extracellular products of  
130 *Aeromonas hydrophila*) so to stimulate an immune response. Carps were fed with the fluorescent  
131 NPs, the biodistribution of which was observed *in vivo* under the fluorescent microscope. A strong  
132 fluorescence given by FITC was detected in the mucous layer of the gut indicating successful  
133 mucoadhesion and permeation of the vaccine loaded CmChNPs [15].

#### 134 *Polysaccharide payloads*

135 Low molecular weight heparin, such as enoxaparin, is an anionic polysaccharide widely used  
136 as an anticoagulant. However, it cannot be orally administered due to its poor penetration through the  
137 GI epithelium [4]. Bagre *et al.* [8] tested the intestinal uptake of enoxaparin loaded in ChNPs coated  
138 with sodium alginate. FITC was employed as a fluorescent marker to track the fate of NPs upon oral  
139 administration to rats. The small intestine was extracted, and a stronger green fluorescence intensity  
140 was observed compared to uncoated NPs, suggesting that the sodium alginate coating increased the  
141 intestinal uptake of NPs. Therefore, the presence of FITC helped to conclude that the alginate coated

142 ChNPs are an adequate carrier for the delivery of enoxaparin through the intestinal epithelium and  
143 enhances the oral bioavailability of this drug. In another study, Fan *et al.* [16] employed FITC to  
144 study the *in vivo* intestinal mucoadhesion of enoxaparin loaded in ChNPs modified with thiol groups  
145 and HPMCP. Following oral administration to rats, confocal images showed a strong green  
146 fluorescence in the small intestine indicating stronger mucoadhesion compared to unmodified NPs.

#### 147 *Chemotherapeutic drugs*

148 Chemotherapeutic drugs generally show low bioavailability upon oral administration. In this  
149 section, we discuss studies in which the use of FITC has assisted in the generation of chitosan-based  
150 nano vectors that can address this issue. Doxorubicin (Dox) is a drug widely used to treat breast,  
151 bladder and other cancers, and is normally IV administrated [17]. The oral bioavailability of Dox is  
152 limited by the efflux transporter P-glycoprotein which recognizes Dox as substrate, limiting its  
153 cellular uptake [17]. Yuan *et al.* [18] employed FITC to track the transport of Dox loaded chitosan  
154 micelles modified with stearic acid, across a monolayer of Caco-2 cells. Tracking the fluorescence  
155 intensity showed that micelles could cross the GI epithelium by micropinocytosis, suggesting that  
156 encapsulating Dox in such micelles can help overcome P-glycoprotein-mediated efflux processes and  
157 thus increase its bioavailability [18]. In another study, a polyelectrolyte complex nanocarrier, made  
158 of chitosan and FITC@CmCh NPs, was employed to deliver Dox to the GI mucosa in rats [10]. FITC  
159 allowed for the examination of the intestinal mucoadhesion of NPs *ex vivo* and a high fluorescence  
160 intensity was found through the entire small intestine indicating suitable drug loaded NPs  
161 biodistribution [10].

162 Curcumin is a polyphenolic compound with several pharmacologic properties, especially  
163 anticancer effects against colon cancer [19]. However, upon oral administration, it is characterized  
164 by poor bioavailability due to the low water solubility and cellular uptake [4]. Khatik *et al.* [20] coated  
165 the surface of curcumin loaded FITC@ChNPs with a pH sensible polymer Eudragit S 100 (Eds) so  
166 to direct NPs to the colon and avoid gastric degradation. A stronger fluorescence was detected in the

167 colon of rats fed with Eds coated NPs compared to uncoated NPs, indicating successful targeting and  
168 uptake of Eds coated curcumin loaded NPs by the colon [20].

### 169 **Concluding remarks**

170 Above, we highlight the recent *in vivo*, *ex vivo* and *in vitro* studies that employed  
171 FITC@ChNPs to study factors involved in bioavailability and uptake of different payloads delivered  
172 orally. Labelling of drug-loaded NPs with FITC allows for tracking and studying them *in vitro* and  
173 *in vivo* in real-time after oral administration. Hence, FITC@ChNPs represent a versatile tool in the  
174 drug delivery arsenal as they can be successfully employed to monitor the fate of ChNPs, and in turn  
175 of the drug, in clinical investigations.

### 176 **Disclaimer Statement**

177 The authors declare no competing financial interests.

### 178 **References**

- 179 1 He, Z. *et al.* (2017) Scalable fabrication of size-controlled chitosan nanoparticles for oral  
180 delivery of insulin. *Biomaterials* 130, 28–41
- 181 2 Du, H. *et al.* (2015) The design of pH-sensitive chitosan-based formulations for  
182 gastrointestinal delivery. *Drug Discov. Today* 20(8), 1004–1011
- 183 3 Ballard, S.T. *et al.* (1995) Regulation of Tight-Junction Permeability During Nutrient  
184 Absorption Across the Intestinal Epithelium. *Annu. Rev. Nutr.* 15, 35–55
- 185 4 Lang, X. *et al.* (2020) Advances and applications of chitosan-based nanomaterials as oral  
186 delivery carriers: A review. *Int. J. Biol. Macromol.* 154, 433–445
- 187 5 Shariatinia, Z. (2019) Pharmaceutical applications of chitosan. *Adv. Colloid Interfac.* 263,  
188 131–194

- 189 6 Collado-González *et al.* (2019) Interaction Between Chitosan and Mucin: Fundamentals and  
190 Applications. *Biomimetics* 4, 32
- 191 7 Su, F.Y. *et al.* (2012) Protease inhibition and absorption enhancement by functional  
192 nanoparticles for effective oral insulin delivery. *Biomaterials* 33, 2801–2811
- 193 8 Bagre, A.P. *et al.* (2013) Alginate coated chitosan core shell nanoparticles for oral delivery of  
194 enoxaparin: in vitro and in vivo assessment. *Int. J. Pharm.* 456, 31–40
- 195 9 Sudhakar, S. *et al.* (2020) Biodistribution and pharmacokinetics of thiolated chitosan  
196 nanoparticles for oral delivery of insulin in vivo. *Int. J. Biol. Macromol.* 150, 281–288
- 197 10 Feng, C. *et al.* (2013) Chitosan/o-carboxymethyl chitosan nanoparticles for efficient and safe  
198 oral anticancer drug delivery: In vitro and in vivo evaluation. *Int. J. Pharm.* 457, 158–167
- 199 11 Zhao, J. and Wu, J. (2006) Preparation and Characterization of the Fluorescent Chitosan  
200 Nanoparticle Probe. *Chinese J. Anal. Chem.* 34, 1555–1559
- 201 12 Wang, J.J. *et al.* (2011) Recent advances of chitosan nanoparticles as drug carriers. *Int. J.*  
202 *Nanomedicine* 6, 765–774
- 203 13 Huang, M. *et al.* (2002) Uptake of FITC-chitosan nanoparticles by A549 cells. *Pharm. Res.*  
204 19, 1488–1494
- 205 14 Makhlof, A. *et al.* (2011) Design and evaluation of novel pH-sensitive chitosan nanoparticles  
206 for oral insulin delivery. *Eur. J. Pharm. Sci.* 42, 445–451
- 207 15 Liu, Y. *et al.* (2012) Preparation and evaluation of oleoyl-carboxymethyl-chitosan (OCMCS)  
208 nanoparticles as oral protein carriers. *J. Mater. Sci. Mater. Med.* 23, 375–384
- 209 16 Fan, B. *et al.* (2016) pH-responsive thiolated chitosan nanoparticles for oral low-molecular  
210 weight heparin delivery: *in vitro* and *in vivo* evaluation. *Int. J. Drug Deliv.* 23, 238–247

- 211 17 Van Der Sandt, I.C.J. *et al.* (2000) Specificity of doxorubicin versus rhodamine-123 in  
212 assessing P-glycoprotein functionality in the LLC-PK1, LLC-PK1:MDR1 and Caco-2 cell  
213 lines. *Eur J of Pharm Sci.* 11(3), 207-214
- 214 18 Yuan, H. *et al.* (2011) Stearic acid-g-chitosan polymeric micelle for oral drug delivery: In  
215 vitro transport and in vivo absorption. *Mol. Pharm.* 8, 225–238
- 216 19 Langner, E. *et al.* (2019) Lycopene, sulforaphane, quercetin, and curcumin applied together  
217 show improved antiproliferative potential in colon cancer cells in vitro. *J. Food Biochem.* 43  
218 (4), e12802
- 219 20 Khatik, R. *et al.* (2013) Colon-specific delivery of curcumin by exploiting Eudragit-  
220 decorated chitosan nanoparticles in vitro and in vivo. *J. Nanoparticle Res.* 15, 1–15

## 221 **FIGURE LEGEND**

222 **Figure 1. (a) The formation of fluorescein isothiocyanate-labelled chitosan nanoparticles**  
223 **(FITC@ChNPs).** Chitosan is tagged with fluorescein isothiocyanate (FITC) via a substitution  
224 reaction, forming FITC-labelled chitosan (FITC@Ch), which contains a thiourea bond (shown in  
225 red). FITC@Ch is then formulated into FITC@ChNPs and loaded with the drug of choice. **(b) The**  
226 **oral administration of drug loaded FITC@ChNPs allows to assess the drug bioavailability over**  
227 **the intestinal epithelium.** FITC@ChNPs are orally administered to rats and following ingestion,  
228 detected in the intestinal epithelium by means of fluorimetry. Owing to chitosan's mucoadhesion  
229 properties, ChNPs can cross the intestinal barrier so that the cargo is released in the blood stream,  
230 increasing its bioavailability.